

Correlations in Complex Systems

Significant Memory Effects Typically Cause Long Time Correlations in Complex Systems

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Glossary

Correlation A correlation describes the degree of relationship between two or more variables. The correlations are viewed due to the impact of random factors and can be characterized by the methods of probability theory.

Correlation function The correlation function (abbreviated, as CF) represents the quantitative measure for the compact description of the wide classes of correlation in the complex systems (CS). The correlation function of two variables in statistical mechanics provides a measure of the mutual order existing between them. It quantifies the way random variables at different positions are correlated. For example in a spin system, it is the thermal average of the scalar product of the spins at two lattice points over all possible orderings.

Memory effects in stochastic processes through correlations Memory effects (abbreviated, as ME) appear at a more detailed level of statistical description of correlation in the hierarchical manner. ME reflect the complicated or hidden character of creation, the propagation and the decay of correlation. ME are produced

by inherent interactions and statistical after-effects in CS. For the statistical systems ME are induced by contracted description of the evolution of the dynamic variables of a CS.

Memory functions Memory functions describe mutual interrelations between the rates of change of random variables on different levels of the statistical description. The role of memory has its roots in the natural sciences since 1906 when the famous Russian mathematician Markov wrote his first paper in the theory of Markov Random Processes. The theory is based on the notion of the instant loss of memory from the prehistory (memoryless property) of random processes.

Information measures of statistical memory in complex systems From the physical point of view time scales of correlation and memory cannot be treated as arbitrary. Therefore, one can introduce some statistical quantifiers for the quantitative comparison of these time scales. They are dimensionless and possess the statistical spectra on the different levels of the statistical description.

Definition of the Subject

As commonly used in probability theory and statistics, a correlation (also so called correlation coefficient), measures the strength and direction of a linear relationship between two random variables. In a more general sense, a correlation or co-relation reflects the deviation of two (or more) variables from mutual independence, although correlation does not imply causation. In this broad sense there are some quantifiers which measures the degree of correlation, suited to the nature of data. Increasing attention has been paid recently to the study of statistical memory effects in random processes that originate from nature by means of non-equilibrium statistical physics. The role of memory has its roots in natural sciences since 1906 when the famous Russian mathematician Markov wrote his first paper on the theory of Markov Random Processes (MRP) [1]. His theory is based on the notion of an instant loss of memory from the prehistory (memoryless property) of random processes. In contrast, there are an abundance of physical phenomena and processes which can be characterized by statistical memory effects: kinetic and relaxation processes in gases [2] and plasma [3], condensed matter physics (liquids [4], solids [5], and superconductivity [6]) astrophysics [7], nuclear physics [8], quantum [9] and classical [9] physics, to name only a few. At present, we have a whole toolbox available of statistical methods which can be efficiently used for the analysis of the memory effects occurring in diverse physical systems. Typical such

schemes are Zwanzig–Mori’s kinetic equations [10,11], generalized master equations and corresponding statistical quantifiers [12,13,14,15,16,17,18], Lee’s recurrence relation method [19,20,21,22,23], the generalized Langevin equation (GLE) [24,25,26,27,28,29], etc.

Here we shall demonstrate that the presence of statistical memory effects is of salient importance for the functioning of the diverse natural complex systems. Particularly, it can imply that the presence of large memory timescales in the stochastic dynamics of discrete time series can characterize catastrophic (or pathological for live systems) violation of salutary dynamic states of CS. As an example, we will demonstrate here that the emergence of strong memory time scales in the chaotic behavior of complex systems (CS) is accompanied by the likely initiation and the existence of catastrophes and crises (Earthquakes, financial crises, cardiac and brain attack, etc.) in many CS and especially by the existence of pathological states (diseases and illness) in living systems.

Introduction

A common definition [30] of a correlation measure $\rho(X, Y)$ between two random variables X and Y with the mean values $E(X)$ and $E(Y)$, and fluctuations $\delta X = X - E(X)$ and $\delta Y = Y - E(Y)$, dispersions $\sigma_X^2 = E(\delta X^2) = E(X^2) - E(X)^2$ and $\sigma_Y^2 = E(\delta Y^2) = E(Y^2) - E(Y)^2$ is defined by:

$$\rho(X, Y) = \frac{E(\delta X \delta Y)}{\sigma_X \sigma_Y},$$

where E is the expected value of the variable. Therefore we can write

$$\rho(X, Y) = \frac{[E(XY) - E(X)E(Y)]}{(E(X^2) - E(X)^2)^{1/2} (E(Y^2) - E(Y)^2)^{1/2}}.$$

Here, a correlation can be defined only if both of the dispersions are finite and both of them are nonzero. Due to the Cauchy–Schwarz inequality, a correlation cannot exceed 1 in absolute value. Consequently, a correlation assumes its maximum at 1 in the case of an increasing linear relationship, or -1 in the case of a decreasing linear relationship, and some value in between in all other cases, indicating the degree of linear dependence between the variables. The closer the coefficient is either to -1 or 1 , the stronger is the correlation between the variables. If the variables are independent then the correlation equals 0, but the converse is not true because the correlation coefficient detects only linear dependencies between two variables.

Since the absolute value of the sample correlation must be less than or equal to 1 the simple formula conveniently suggests a single-pass algorithm for calculating sample correlations. The square of the sample correlation coefficient, which is also known as the coefficient of determination, is the fraction of the variance in σ_x that is accounted for by a linear fit of x_i to σ_y . This is written

$$R_{xy}^2 = 1 - \frac{\sigma_{y|x}^2}{\sigma_y^2},$$

where $\sigma_{y|x}^2$ denotes the square of the error of a linear regression of x_i on y_i in the equation $y = a + bx$,

$$\sigma_{y|x}^2 = \frac{1}{n} \sum_{i=1}^n (y_i - a - bx_i)^2$$

and σ_y^2 denotes just the dispersion of y .

Note that since the sample correlation coefficient is symmetric in x_i and y_i , we will obtain the same value for a fit to y_i :

$$R_{xy}^2 = 1 - \frac{\sigma_{x|y}^2}{\sigma_x^2}.$$

This equation also gives an intuitive idea of the correlation coefficient for random (vector) variables of higher dimension. Just as the above described sample correlation coefficient is the fraction of variance accounted for by the fit of a 1-dimensional linear submanifold to a set of 2-dimensional vectors (x_i, y_i) , so we can define a correlation coefficient for a fit of an m -dimensional linear submanifold to a set of n -dimensional vectors. For example, if we fit a plane $z = a + bx + cy$ to a set of data (x_i, y_i, z_i) then the correlation coefficient of z to x and y is

$$R^2 = 1 - \frac{\sigma_{z|xy}^2}{\sigma_z^2}.$$

Correlation and Memory in Discrete Non-Markov Stochastic Processes

Here we present a non-Markov approach [31,32] for the study of long-time correlations in chaotic long-time dynamics of CS. For example, let the variable x_i be defined as the R-R interval or the time distance between nearest, so called R peaks occurring in a human electrocardiogram (ECG). The generalization will consist in taking into account non-stationarity of stochastic processes and its further applications to the analysis of the heart-rate variability.

We should bear in mind, that one of the key moments of the spectral approach in the analysis of stochastic processes consists in the use of normalized time correlation function (TCF)

$$a_0(t) = \frac{\langle\langle \mathbf{A}(T) \mathbf{A}(T+t) \rangle\rangle}{\langle \mathbf{A}(T)^2 \rangle}. \quad (1)$$

Here the time T indicates the beginning of a time serial, $\mathbf{A}(t)$ is a state vector of a complex system as defined below in Eq. (5) at t , $|\mathbf{A}(t)|$ is the length of vector $\mathbf{A}(t)$, the double angular brackets indicate a scalar product of vectors and an ensemble averaging. The ensemble averaging is, of course needed in Eq. (1) when correlation and other characteristic functions are constructed. The average and scalar product becomes equivalent when a vector is composed of elements from a discrete-time sampling, as done later. Here a continuous formalism is discussed for convenience. However further, since Sect. ‘‘Correlation and Memory in Discrete Non-Markov Stochastic Processes’’ we shall consider only a case of discrete processes.

The above-stated designation is true only for stationary systems. In a non-stationary case Eq. (1) is not true and should be changed. The concept of TCF can be generalized in case of discrete non-stationary sequence of signals. For this purpose the standard definition of the correlation coefficient in probability theory for the two random signals X and Y must be taken into account

$$\rho = \frac{\langle\langle \mathbf{X}\mathbf{Y} \rangle\rangle}{\sigma_X \sigma_Y}, \quad \sigma_X = \langle|\mathbf{X}|\rangle, \quad \sigma_Y = \langle|\mathbf{Y}|\rangle. \quad (2)$$

In Eq. (2) the multi-component vectors \mathbf{X} , \mathbf{Y} are determined by fluctuations of signals x and y accordingly, σ_X^2, σ_Y^2 represent the dispersions of signals \mathbf{x} and \mathbf{y} , and values $|\mathbf{X}|, |\mathbf{Y}|$ represent the lengths of vectors \mathbf{X} , \mathbf{Y} , correspondingly. Therefore, the function

$$a(T, t) = \frac{\langle\langle \mathbf{A}(T) \mathbf{A}(T+t) \rangle\rangle}{\langle|\mathbf{A}(T)|\rangle \langle|\mathbf{A}(T+t)|\rangle} \quad (3)$$

can serve as the generalization of the concept of TCF (1) for non-stationary processes $\mathbf{A}(T+t)$. The non-stationary TCF (3) obeys the conditions of the normalization and attenuation of correlation

$$a(T, 0) = 1, \quad \lim_{t \rightarrow \infty} a(T, t) = 0.$$

Let us note, that in a real CS the second limit, typically, is not carried out due possible occurrence nonergodicity (meaning that a time average does not equal its ensemble average). According to the Eqs. (1) and (3) for the quantitative description of non-stationarity it is convenient to

introduce a function of non-stationarity

$$\gamma(T, t) = \frac{\langle|\mathbf{A}(T+t)|\rangle}{\langle|\mathbf{A}(T)|\rangle} = \left\{ \frac{\sigma^2(T+t)}{\sigma^2(T)} \right\}^{1/2}. \quad (4)$$

One can see that this function equals the ratio of the lengths of vectors of final and initial states. In case of stationary process the dispersion does not vary with the time (or its variation is very weak). Therefore the following relations

$$\sigma(T+t) = \sigma(T), \quad \gamma(T, t) = 1 \quad (5)$$

hold true for the stationary process.

Due to the condition (5) the following function

$$\Gamma(T, t) = 1 - \gamma(T, t) \quad (6)$$

is suitable in providing a dynamic parameter of non-stationarity. This dynamic parameter can serve as a quantitative measure of non-stationarity of the process under investigation. According to Eqs. (4)–(6) it is reasonable to suggest the existence of three different elementary classes of non-stationarity

$$|\Gamma(T, t)| = |1 - \gamma(T, t)| = \begin{cases} \ll 1, & \text{weak non-stationarity} \\ \sim 1, & \text{intermediate non-stationarity} \\ \gg 1, & \text{strong non-stationarity} \end{cases}. \quad (7)$$

The existence of dynamic parameter of non-stationarity makes it possible to determine, on-principle, the type of non-stationarity of the underlying process and to find its spectral characteristics from the experimental data base. We intend to use Eqs. (4), (6), (7) for the quantitative description of effects of non-stationarity in the investigated temporary series of R-R intervals of human ECG’s for healthy people and patients after myocardial infarction (MI).

Statistical Theory of Non-Stationary Discrete Non-Markov Processes in Complex Systems

Here we shall extend the original results of the statistical theory of discrete non-Markov processes in complex systems, developed recently in [31], for the case of non-stationary processes. The theory [31] is developed on the basis of first principles and represents a discrete finite-difference analogy for complex systems of well known Zwanzig–Mori’s kinetic equations [10,11,12,13,14,15,16,17,18] used in the statistical physics of condensed matter.

We examine a discrete stochastic process $X(T + t)$, where $t = m\tau$

$$X = \{x(T), x(T + \tau), x(T + 2\tau), \dots, x(T + k\tau), \dots, x(T + (N - 1)\tau)\}, \quad (8)$$

where T is the beginning of the time and τ is a discretization time. The normalized time correlation function (TCF)

$$a(t) = \frac{1}{(N - m)\sigma^2} \sum_{j=0}^{N-1-m} \delta x(T + j\tau) \delta x(T + (j + m)\tau) \quad (9)$$

yields a convenient measure to analyze the dynamic properties of complex systems. Herein, we used the variance σ^2 , the fluctuation $\delta x(T + j\tau)$, which in terms of the mean value $\langle x \rangle$ reads:

$$\delta x_j = \delta x(T + j\tau) = x(T + j\tau) - \langle x \rangle, \quad (10)$$

$$\sigma^2 = \frac{1}{(N - m)} \sum_{j=0}^{N-1-m} \{\delta x(T + j\tau)\}^2,$$

$$\langle x \rangle = \frac{1}{(N - m)} \sum_{j=0}^{N-1-m} x(T + j\tau). \quad (11)$$

The discrete time t is given as $t = m\tau$.

In general, the mean value, the variance and TCF in (9), (10) and (11) is dependent on the numbers m and N . All indicated values cease to depend on numbers m and N for stationary processes when $m \ll N$. The definition of TCF in Eq. (9) is true only for stationary processes.

Next, we shall try to take into account this important dependence. With this purpose we shall form two k -dimensional vectors of state by the process (8):

$$\mathbf{A}_k^0 = (\delta x_0, \delta x_1, \delta x_2, \dots, \delta x_{k-1}), \quad (12)$$

$$\mathbf{A}_{m+k}^m = (\delta x_m, \delta x_{m+1}, \delta x_{m+2}, \dots, \delta x_{m+k-1}).$$

When a vector of a state is composed of elements from a discrete-time sampling, the average and scalar product in Eq. (1) become equivalent. In an Euclidean space of vectors of state (12) TCF $a(t)$

$$a(t) = \frac{\langle \mathbf{A}_{N-1-m}^0 \mathbf{A}_{N-1}^m \rangle}{(N - m)\{\sigma(N - m)\}^2} = \frac{\langle \mathbf{A}_{N-1-m}^0 \mathbf{A}_{N-1}^m \rangle}{|\mathbf{A}_{N-1-m}^0|^2} \quad (13)$$

describes the correlation of two different states of the system ($t = m\tau$). Here the brackets $\langle \dots \rangle$ indicate the scalar product of the two vectors. The dimension dependence of the corresponding vectors is also taken into account

in the variance $\sigma = \sigma(N - m)$. As a matter of fact TCF $a(t) = \cos \vartheta$, where ϑ is the angle between the two vectors from Eq. (12). Let's introduce a unit vector of dimension $(N - m)$ in the following way:

$$\mathbf{n} = \frac{\mathbf{A}_{N-1-m}^0}{\sqrt{(N - m)\sigma^2}}. \quad (14)$$

Then, the TCF $a(t)$ (9) is given by

$$a(t) = \langle \mathbf{n}(0) \mathbf{n}(t) \rangle. \quad (15)$$

From the above discussion it is evident that Eqs. (13)–(15) are true for the stationary processes only. In case of non-stationary processes it is necessary to redefine TCF, taking into account the non-stationarity in the variance σ^2 in a line with Eqs.(2)–(7). For this purpose we shall redefine a unit vector of the final state as following

$$\mathbf{n}(t) = \frac{\mathbf{A}_{N-1}^m(t)}{|\mathbf{A}_{N-1}^m(t)|}. \quad (16)$$

For non-stationary processes it is convenient to write the TCF as the scalar product of the two unit vectors of the initial and final states

$$a(t) = \langle \mathbf{n}(0) \mathbf{n}(t) \rangle = \frac{\langle \mathbf{A}_{N-1-m}^0(0) \mathbf{A}_{N-1}^m(t) \rangle}{|\mathbf{A}_{N-1-m}^0(0)| |\mathbf{A}_{N-1}^m(t)|}. \quad (17)$$

Now we shall turn to the the dynamics of a non-stationary stochastic process. The equation of motion of a the random process x_j can be written in a finite-difference form for $0 \leq j \leq N - 1$ [15] in the following way

$$\frac{dx_j}{dt} \Rightarrow \frac{\Delta \delta x_j}{\Delta t} = \frac{\delta x_j(t + \tau) - \delta x_j(t)}{\tau}. \quad (18)$$

Then it is convenient to define the discrete evolution single step operator \hat{U} as following:

$$x(T + (j + 1)\tau) = \hat{U}(T + (j + 1)\tau, T + j\tau) x(T + j\tau). \quad (19)$$

In the case of stationary process we can rewrite the equation of motion (18) in a more simple form

$$\frac{\Delta \delta x_j}{\Delta t} = \tau^{-1} \{\hat{U}(\tau) - 1\} \delta x_j. \quad (20)$$

The invariance of the mean value $\langle x \rangle$ is taken into account in an Eq. (20)

$$\langle x \rangle = \hat{U}(\tau) \langle x \rangle, \quad \{\hat{U}(\tau) - 1\} \langle x \rangle = 0. \quad (21)$$

In case of a non-stationary process it is necessary to turn to the equation of motion for vector of the final state $\mathbf{A}_{m+k}^m(t)$ ($k = N - 1 - m$)

$$\frac{\Delta \mathbf{A}_{m+k}^m(t)}{\Delta t} = i\hat{L}(t, \tau) \mathbf{A}_{m+k}^m(t), \quad (22)$$


326 where Liouville's quasioperator is


$$327 \quad \hat{L}(t, \tau) = (i\tau)^{-1} \{ \hat{U}(t + \tau, t) - 1 \}. \quad (23)$$

328 It is well known that, in general, a stochastic trajec-
329 tory does not obey a linear equation, so the general evolu-
330 tion operator and Liouville's quasioperator should prob-
331 ably be non-linear. Furthermore, in statistical physics the
332 Liouville's operator acts upon the probability densities of
333 dynamical variables, as well upon the variables itself like
334 in Mori's paper [12]. The evolution of the density would
335 be indeed linear. But Mori used the Liouville operator
336 in the quantum equation of motion in [12]. In line with
337 Mori [12] Eqs. (20), (22) can be considered as formal and
338 exact equations of the motion of a complex system.

339 Thus, due to the Eqs. (17), (22) and (23) we may take
340 into account the non-stationarity of the stochastic process.
341 Towards this goal let's introduce the linear projection op-
342 erator in Euclidean space of the state vectors

$$343 \quad \Pi \mathbf{A}(t) = \frac{\mathbf{A}(0) \langle \mathbf{A}(0) | \mathbf{A}(t) \rangle}{|\mathbf{A}(0)|^2}, \quad \Pi = \frac{\mathbf{A}(0) \langle \mathbf{A}(0) |}{\langle \mathbf{A}(0) | \mathbf{A}(0) \rangle}, \quad (24)$$

344 where angular brackets in numerator present the bound-
345 aries of action for the scalar product. 

346 For the analyzing the dynamics  of the stochastic
347 process $\mathbf{A}(t)$ the vector $\mathbf{A}_k^0(0)$ from (12) can be considered
348 as a vector of the initial state $\mathbf{A}(0)$, and vector $\mathbf{A}_{m+k}^m(t)$
349 from (12) at value $m+k = N-1$ can be considered as
350 the vector of the final state $\mathbf{A}(t)$.

351 It is necessary to note that the projection operator (24)
352 has the required property of idem-potency $\Pi^2 = \Pi$. The
353 presence of operator Π allows one to introduce the mutu-
354 ally supplementary projection operator P :

$$355 \quad P = 1 - \Pi, \quad P^2 = P, \quad \Pi P = P \Pi = 0. \quad (25)$$

356 It is necessary to remark, that both projectors Π and P are
357 linear and can be recorded for the fulfillment of operations
358 in the particular Euclidean space. Due to the property (17)
359 and Eq. (4) it is easy to obtain the required TCF:

$$360 \quad \begin{aligned} \Pi \mathbf{A}(t) &= \Pi \mathbf{A}_{m+k}^m(t) \\ &= \mathbf{A}_k^0(0) \langle \mathbf{n}_k^0(0) | \mathbf{n}_{k+m}^m(t) \rangle \gamma_1(t) \\ &= \mathbf{A}_k^0(0) a(t) \gamma_1(t), \end{aligned} \quad (26)$$

$$361 \quad \gamma_1(t) = \frac{|\mathbf{A}_{m+k}^m(t)|}{|\mathbf{A}_k^0(0)|}.$$

362 Therefore the projector Π generates a unit vector along
363 the vector of the final state $\mathbf{A}(t)$ and makes its projection
364 onto the initial state vector $\mathbf{A}(0)$.

365 The existence of a pair of two mutually supplementary
projection operators Π and P allows one to carry out the

366 splitting of Euclidean space of vectors $A(\mathbf{A}(0), \mathbf{A}(t) \in A)$
367 into a straight sum of two mutually supplementary sub-
368 spaces in the following way

$$A = A' + A'', \quad A' = \Pi A, \quad A'' = PA. \quad (27)$$

370 Substituting Eq. (27) in Eq. (23) we find Liouville's
371 quasioperator \hat{L} in a matrix form

$$372 \quad \hat{L} = \hat{L}_{11} + \hat{L}_{12} + \hat{L}_{21} + \hat{L}_{22}, \quad (28)$$

373 where the matrix elements are introduced

$$374 \quad \begin{aligned} \hat{L}_{11} &= \Pi \hat{L} \Pi, \quad \hat{L}_{12} = \Pi \hat{L} P, \\ \hat{L}_{21} &= P \hat{L} \Pi, \quad \hat{L}_{22} = P \hat{L} P. \end{aligned} \quad (29)$$

375 The Euclidean space of values of Liouville's quasiop-
376 erator $W = \hat{L}A$ will be generated by the vectors \mathbf{W} of di-
377 mension $k-1$


$$378 \quad \begin{aligned} (\mathbf{W}(0) \in W, \mathbf{W}(t) \in W) \\ W = W' + W'', \quad W' = \Pi W, \quad W'' = PW. \end{aligned} \quad (30)$$

379 Matrix elements \hat{L}_{ij} of the contracted description

$$380 \quad \hat{L} = \begin{pmatrix} \hat{L}_{11} & \hat{L}_{12} \\ \hat{L}_{21} & \hat{L}_{22} \end{pmatrix} \quad (31)$$

381 are acting in the following way:

$$382 \quad \begin{aligned} \hat{L}_{11} &- \text{from a subspace } A' \text{ to subspace } W', \\ \hat{L}_{12} &- \text{from } A'' \text{ to } W', \\ \hat{L}_{21} &- \text{from } W' \text{ to } W'' \text{ and} \\ \hat{L}_{22} &- \text{from } A'' \text{ to } W''. \end{aligned}$$

383 The projection operators Π and P provide the con-
384 tracted description of the stochastic process. Splitting the
385 dynamic Eq. (22) into two equations in the two mutually
386 supplementary Euclidean subspaces (see, for example [11]
387 , we find

$$388 \quad \frac{\Delta \mathbf{A}'(t)}{\Delta t} = i \hat{L}_{11} \mathbf{A}'(t) + i \hat{L}_{12} \mathbf{A}''(t), \quad (32)$$

$$389 \quad \frac{\Delta \mathbf{A}''(t)}{\Delta t} = i \hat{L}_{21} \mathbf{A}'(t) + i \hat{L}_{22} \mathbf{A}''(t). \quad (33)$$

390 Following [31,32] it is necessary to eliminate first
391 the irrelevant part $\mathbf{A}''(t)$ in order to simplify Liouville's
392 Eq. (22) and then to write a closed equation for relevant
393 part $\mathbf{A}'(t)$. According to [32] that can be achieved by a se-
394 ries of successive steps (for example, see Eqs. (32)–(36)

395 in [32]). First a solution to Eq. (33) for the first step can
396 be obtained in a form

$$\begin{aligned}
\frac{\Delta \mathbf{A}''(t)}{\Delta t} &= \frac{\mathbf{A}''(t + \tau) - \mathbf{A}''(t)}{\tau} \\
&= i\hat{L}_{21} \mathbf{A}'(t) + i\hat{L}_{22} \mathbf{A}''(t), \\
\mathbf{A}''(t + \tau) &= \mathbf{A}''(t) + i\tau \hat{L}_{21} \mathbf{A}'(t) + i\tau \hat{L}_{22} \mathbf{A}''(t) \\
&= \{1 + i\tau \hat{L}_{22}\} \mathbf{A}''(t) + i\tau \hat{L}_{21} \mathbf{A}'(t) \\
&= U_{22}(t + \tau, t) \mathbf{A}''(t) + i\tau \hat{L}_{21}(t + \tau, t) \mathbf{A}'(t).
\end{aligned}
\tag{34}$$

398 We next can derive a finite-difference kinetic equation
399 of a non-Markov type for TCF $a(t = m\tau)$

$$\frac{\Delta a(t)}{\Delta t} = \lambda_1 a(t) - \tau \Lambda_1 \sum_{j=0}^{m-1} M_1(t - j\tau) a(j\tau). \tag{35}$$

401 Here, λ_1 is a eigenvalue, Λ_1 is a relaxation parameter
402 of Liouville's quasioperator \hat{L}

$$\begin{aligned}
\lambda_1 &= i \frac{\langle \mathbf{A}_k^0(0) | \hat{L} \mathbf{A}_k^0(0) \rangle}{|\mathbf{A}_k^0(0)|^2}, \\
\Lambda_1 &= \frac{\langle \mathbf{A}_k^0(0) | \hat{L}_{12} \hat{L}_{21} \mathbf{A}_k^0(0) \rangle}{|\mathbf{A}_k^0(0)|^2} = \frac{\langle \mathbf{A}_k^0(0) | \hat{L}^2 \mathbf{A}_k^0(0) \rangle}{|\mathbf{A}_k^0(0)|^2},
\end{aligned}
\tag{36}$$

404 The angular brackets indicate here a scalar product of
405 new state vectors. Function $M_1(t - j\tau)$ on the right side of
406 Eq. (35) represents a modified memory function (MF) of
407 the first order

$$M_1(t - j\tau) = \frac{\gamma_1(t - j\tau)}{\gamma_1(t)} m_1(t - j\tau). \tag{37}$$

409 For stationary processes the function $\gamma_1(t)$ approaches
410 unity. Then the memory functions $M_1(t)$ and $m_1(t)$ co-
411 incide with each other. The latter equation is the first ki-
412 netic finite-difference equation for TCF. It is remarkable,
413 that the non-Markovity, discretization and non-stationar-
414 ity of stochastic process can be considered explicitly. Due
415 to the presence of non-stationarity both in TCF and in the
416 first memory function this equation generalizes our results
417 recently obtained in [31].

418 Following the projection technique described above,
419 we arrive at a chain of connected kinetic finite-difference
420 equations of a non-Markov type for the normalized short
421 memory functions $m_n(t)$ in Euclidean space of state vec-

tors of dimension $(k - n)$ ($t = m\tau, n \geq 1$)

$$\begin{aligned}
\frac{\Delta m_n(t)}{\Delta t} &= \lambda_{n+1} m_n(t) - \tau \Lambda_{n+1} \\
&\times \sum_{j=0}^{m-1} m_{n+1}(j\tau) m_n(t - j\tau) \\
&\times \left\{ \frac{\gamma_{n+1}(j\tau) \gamma_{n+1}(t - j\tau)}{\gamma_n(t)} \right\},
\end{aligned}
\tag{38}$$

$$m_{n+1}(t) = \frac{\langle \mathbf{W}_{n+1}(0) | \mathbf{W}_{n+1}(t) \rangle}{|\mathbf{W}_{n+1}(0)| |\mathbf{W}_{n+1}(t)|},$$

$$\gamma_n(j\tau) = \left\{ \frac{|\mathbf{W}_n(j\tau)|}{|\mathbf{W}_n(0)|} \right\}. \tag{39}$$

423 Here, $\gamma_n(j\tau)$ is the n th order of the non-stationarity func-
424 tion.

425 The set of all memory functions $m_1(t), m_2(t), m_3(t), \dots$
426 allows one to describe non-Markov processes and statisti-
427 cal memory effects in the considered non-stationary
428 system. For the particular case we obtain a more simple
429 form for the set of equations for the first three short
430 memory functions, namely ($t = m\tau$):

$$\begin{aligned}
\frac{\Delta a(t)}{\Delta t} &= -\tau \Lambda_1 \sum_{j=0}^{m-1} m_1(j\tau) \left\{ \frac{\gamma_1(j\tau) \gamma_1(t - j\tau)}{\gamma_1(t)} \right\} \\
&\times a(t - j\tau) + \lambda_1 a(t),
\end{aligned}$$

$$\frac{\Delta m_1(t)}{\Delta t} = -\tau \Lambda_2 \sum_{j=0}^{m-1} m_2(j\tau) \left\{ \frac{\gamma_2(j\tau) \gamma_2(t - j\tau)}{\gamma_2(t)} \right\} \tag{40}$$

$$\times m_1(t - j\tau) + \lambda_2 m_1(t),$$

$$\frac{\Delta m_2(t)}{\Delta t} = -\tau \Lambda_3 \sum_{j=0}^{m-1} m_3(j\tau) \left\{ \frac{\gamma_3(j\tau) \gamma_3(t - j\tau)}{\gamma_3(t)} \right\}$$

$$\times m_2(t - j\tau) + \lambda_3 m_2(t).$$

434 Here the relaxation parameters Λ_1, Λ_2 and Λ_3 have al-
435 ready been determined and the non-stationarity functions
436 $\gamma_n(t)$ have been introduced earlier. By analogy with Eq. (6)
437 we can introduce a set of dynamic parameters of non-sta-
438 tionarity (PNS) for the arbitrary n th relaxation level

$$\Gamma_n(T, t) = 1 - \gamma_n(t) = 1 - \gamma_n(T, t). \tag{41}$$

439 The whole set of values of dynamic PNS $\gamma_n(t)$ determines
440 the broad spectrum of non-stationarity effects of the con-
441 sidered process.

442 The obtained equations are similar to the well known
443 Zwanzig-Mori's kinetic equations [10,11,12,13,14,15,16,
444 17,18] used in non-equilibrium statistical physics of con-
445 densed matters. Let us point out three essential distinc-
446 tions of our Eqs. (40) from the results in [10,11,12]. In
447

Zwanzig–Mori’s theory the key moment in the analysis of considered physical systems is the presence of a Hamiltonian and an operation of a statistical averaging carried out with the help of quantum density operator or classic Gibbs distribution function [33]. In our examined case, both the Hamiltonian and the distribution function are absent. There are exact classic or quantum equations of motion in physics; so Liouville’s equation and Liouville’s operator are useful in many applications. The motion of individual particles and whole statistic system is described by variables varying in continuous time. Therefore, for physical systems it is possible to use effectively the methods of integro-differential calculus, based on the mathematically accustomed (but from the physical point of view difficult for understanding) representation of infinitesimal variations of values of coordinates and time. By nature, the monitored time evolution of most complex systems is discrete. As well known, discretization is inherent in a wide variety both of classical and quantum complex systems. This forces us to abandon the concept of an infinite small values and continuity and instead turn to discrete-difference schemes. And, at last, the third feature is connected with incorporating the issue of non-stationary processes into our theory. The Zwanzig–Mori theory is typically applied only for stationary processes. Due to the introduction of normalized vectors of states and the use of the appropriate projection technique [13] our theory allows to take into account non-stationary processes as well. The latter ones can be described by the non-Markov kinetic equations together with the introduction of the set of non-stationarity functions.

The non-stationary theory [32] put forward here differs from the stationary case [31]. The external structure of the kinetic equations remains invariant; they represent the kinetic equations with memory. However, the functions and the parameters, which are included in these equations, appreciably differ from each other. As we already remarked above, non-stationarity effects enter both, in the functions $\gamma_n(t)$ and in spectral and kinetic parameters.

Correlation and Memory in Discrete Non-Markov Stochastic Processes Generated by Random Events

Here we shall find a chain of the kinetic interconnected finite-difference equations for a discrete correlation function $a(n)$ and memory functions $M_s(n)$ in the linear scale of events $E = \{\xi_1, \xi_2, \xi_3, \dots, \xi_N\}$.

The Basic Assumptions and Concepts of the Theory of Discrete Non-Markov Stochastic Processes of the Events Correlations

As an example we shall consider the time variations of the total X-ray flux of an astrophysical object at a succession of events:

$$E = \{\xi_1, \xi_2, \xi_3, \dots, \xi_k, \dots, \xi_N\}, \quad (42)$$

where ξ_i is an event, which occurs at time instant t_i , where $i = 1, \dots, N$ counts the event number.

The average value $\langle E \rangle$, fluctuations $\delta\xi$ and dispersion σ^2 for the set of N events are obtained as:

$$\begin{aligned} \langle E \rangle &= \frac{1}{N} \sum_{i=1}^N \xi_i, \delta\xi_i = \xi_i - \langle E \rangle, \\ \sigma^2 &= \frac{1}{N} \sum_{i=1}^N \delta\xi_i^2 = \frac{1}{N} \sum_{i=1}^N \{\xi_i - \langle E \rangle\}^2. \end{aligned} \quad (43)$$

According to [35,36,37,38], for the description of the dynamical properties of the studied system we introduce the correlation dependence of the discrete set of events (see Eq. (42)) using the CF:

$$a(n) = \frac{1}{(N-m)\sigma^2} \sum_{i=1}^{N-m} \delta\xi_i \delta\xi_{i+m}. \quad (44)$$

Here $n = m\Delta n$, $\Delta n = 1$ is the discretization step. The function $a(n)$, which emerges in this way, is the “event” correlation function (ECF). The normalized ECF must obey the conditions of normalization and of the attenuation of correlation, i. e.: $\lim_{n \rightarrow 1} a(n) = 1$, $\lim_{n \rightarrow \infty} a(n) = 0$. We remark, however, that the second condition for the case the physical complex systems is typically not observed (at $N \gg 0$). It is necessary to note that in [18] the correlation function for the aftershock events has been introduced:

$$C(n + n_W, n_W) = \frac{[(\langle t_{n+n_W} t_{n_W} \rangle) - \langle t_{n+n_W} \rangle \langle t_{n_W} \rangle]}{(\sigma_{n+n_W}^2 \sigma_{n_W}^2)^{1/2}},$$

where the averages and the variance are given by

$$\begin{aligned} \langle t_m \rangle &= \frac{1}{N} \sum_{k=0}^{N-1} t_{m+k}, \\ \langle t_m t'_m \rangle &= \frac{1}{N} \sum_{k=0}^{N-1} t_{m+k} t'_{m+k}, \text{ and} \\ \sigma_m^2 &= \langle t_m^2 \rangle - \langle t_m \rangle^2, \end{aligned}$$

respectively.

524 By the direct analogy of [31,32,35] we use the fi-
525 nite-difference Liouville's equation of motion in the event
526 scale for describing the evolution of discrete set of events
527 Eq. (11), (13):

$$528 \quad \frac{\Delta \xi_i(n)}{\Delta n} = i \widehat{L}(n, 1) \xi_i(n). \quad (45)$$

529 Here $\xi_i(n+1) = U(n+1, n) \xi_i(n)$, $U(n+1, n)$ is the
530 "event" evolution operator. It determines the shift in
531 linear event scale to one step Δn . The evolution op-
532 erator $U(n+1, n)$ and Liouville's quasioperator $\widehat{L}(n, 1)$
533 can be made explicit by writing: $\widehat{L}(n, 1) = (i\Delta n)^{-1} (U(n$
534 $+1, n) - 1)$.

535 Let's represent the set of values of the dynamical vari-
536 able $\delta \xi_j = \delta \xi(j\Delta n)$, $j = 1, \dots, N$ as the k -component
537 vector of system state in linear Euclidean space:

538 a) the vector of initial state of studied complex system:

$$539 \quad \mathbf{A}_k^1 = \{\delta \xi_1, \delta \xi_2, \delta \xi_3, \dots, \delta \xi_k\}, \quad (46)$$

540 b) the vector of final system's state, which is shifted on
541 the m events along the event scale:

$$542 \quad \mathbf{A}_{m+k}^m = \{\delta \xi_{m+1}, \delta \xi_{m+2}, \delta \xi_{m+3}, \dots, \delta \xi_{m+k}\}, \quad (47)$$

543 where $1 \leq k \leq N$. The vectors of initial and final states,
544 which are submitted in a similar way, are very conven-
545 nient for analyzing the dynamics of the observed dis-
546 crete stochastic processes with the help of discrete non-
547 Markov processes.

548 To represent the ECF in a more compact form, we
549 use the expression for the scalar product of vectors
550 $\langle \mathbf{A}_k^1 \cdot \mathbf{A}_{m+k}^m \rangle = \sum_{j=1}^k A_j^1 A_{m+j}^m$, and the Eqs. (64)
551 and (65) TS6:

$$552 \quad a(n) = \frac{\langle \mathbf{A}_k^1(1) \mathbf{A}_{m+k}^m(n) \rangle}{\langle |\mathbf{A}_k^1(1)|^2 \rangle}. \quad (48)$$

553 Construction of Chain of Finite-Difference Non- 554 Markov Kinetic Equations for the Events Correlation

555 Let us consider the finite-difference Liouville's equation
556 (Eq. (44)) for the vector of final system states:

$$557 \quad \frac{\Delta \mathbf{A}_{m+k}^m(n)}{\Delta n} = i \widehat{L}(n, 1) \mathbf{A}_{m+k}^m(n). \quad (49)$$

558 We introduce the projection operator Π , which
559 projects the final vector $\mathbf{A}_{m+k}^m(n)$ on the direction of ini-
560 tial vector, and also the orthogonal operator P. The op-
561 erators Π and P possess the following properties: $\Pi =$
562 $|\mathbf{A}_k^1(1)\rangle \langle \mathbf{A}_k^1(1)| / \langle |\mathbf{A}_k^1(1)|^2 \rangle$, $\Pi^2 = \Pi$, $P = 1 - \Pi$, $P^2 = P$,

563 $\Pi P = P \Pi = 0$. They are idempotent and mutually com-
564plementary.

565 The initial ECF $a(n)$ (Eq. (48)) can be derived by means
566 of projecting the vector of final states $\mathbf{A}_{m+k}^m(n)$ on the vec-
567 tor of initial state $\mathbf{A}_k^1(1)$:

$$568 \quad \Pi \mathbf{A}_{m+k}^m(n) = \frac{\mathbf{A}_k^1(1) \langle \mathbf{A}_k^1(1) \mathbf{A}_{m+k}^m(n) \rangle}{\langle |\mathbf{A}_k^1(1)|^2 \rangle} = \mathbf{A}_k^1(1) a(n). \quad (50)$$

569 The operators Π and P split Euclidean vector space
570 $A(k)$ into two mutually orthogonal subspaces:

$$571 \quad \begin{aligned} A(k) &= A'(k) + A''(k), & A'(k) &= \Pi A(k), \\ A''(k) &= P A(k), & \mathbf{A}_{m+k}^m &\in A(k). \end{aligned} \quad (51)$$

572 As a result the finite-difference Liouville's Eq. (67) TS6
573 can be represented as a system of 2 equations into mutually
574 orthogonal linear subspaces:

$$575 \quad \frac{\Delta A'(n)}{\Delta n} = i \widehat{L}_{11} A'(n) + i \widehat{L}_{12} A''(n), \quad (52)$$

$$576 \quad \frac{\Delta A''(n)}{\Delta n} = i \widehat{L}_{21} A'(n) + i \widehat{L}_{22} A''(n). \quad (53)$$

577 Here $\widehat{L}_{ij} = \Pi_i \widehat{L} \Pi_j$ are the matrix elements of Liou-
578 ville's quasioperator:

$$579 \quad \begin{aligned} \widehat{L} &= \widehat{L}_{11} + \widehat{L}_{12} + \widehat{L}_{21} + \widehat{L}_{22}, \\ \widehat{L}_{11} &= \Pi \widehat{L} \Pi, & \widehat{L}_{12} &= \Pi \widehat{L} P, \\ \widehat{L}_{21} &= P \widehat{L} \Pi, & \widehat{L}_{22} &= P \widehat{L} P. \end{aligned} \quad (54)$$

580 To solve the system of Eqs. (52), (53) TS6 we eliminate
581 the non-reducible part, which contains $A''(n)$ and derive
582 the self-contained equation for the reducible part $A'(n)$. In
583 doing so we solve the Eq. (52) step-by-step and shall sub-
584 stitute the obtained solution into the Eq. (53). As a result
585 we arrive at the closed kinetic equation:

$$586 \quad \begin{aligned} \frac{\Delta A'(n+m\Delta n)}{\Delta n} &= i \widehat{L}_{11} A'(n+m\Delta n) \\ &+ i \widehat{L}_{12} \{1 + i\Delta n \widehat{L}_{22}\}^m A''(n) \\ &- \widehat{L}_{12} \sum_{j=1}^m \{1 + i\Delta n \widehat{L}_{22}\}^j \Delta n \\ &\times \widehat{L}_{21} A'(n + [m-j]\Delta n). \end{aligned} \quad (55)$$

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588 By use of projection operators Π and P we found the
589 closed finite-difference kinetic equation of non-Markov
590 type for the initial ECF:

$$\frac{\Delta a(n)}{\Delta n} = i\lambda_1 a(n) - \Delta n \Lambda_1 \sum_{j=1}^m M_1(j\Delta n) a(n-j\Delta n). \quad (56)$$

591
592 As $\Delta n = 1$, solution of the last equation must be fol-
593 lowing:

$$594 \quad a(n+1) = \{i\lambda_1 + 1\} a(n) - \Lambda_1 \sum_{j=1}^m M_1(j) a(n-j). \quad (57)$$

595 Here λ_1 is the proper value of Liouville's quasiopera-
596 tor \widehat{L} , Λ_1 is the relaxation parameter, which dimension is
597 square of frequency, $M_1(j\Delta n)$ is the normalized memory
598 function of the first order:

$$\lambda_1 = \frac{\langle A_k^1(1) \widehat{L} A_k^1(1) \rangle}{\langle |A_k^1(1)|^2 \rangle},$$

$$599 \quad \Lambda_1 = \frac{\langle A_k^1 \widehat{L}_{12} \widehat{L}_{21} A_k^1(1) \rangle}{\langle |A_k^1(1)|^2 \rangle},$$

$$M_1(j\Delta n) = \frac{\langle A_k^1(1) \widehat{L}_{12} (1 + i\Delta n \widehat{L}_{22})^j \widehat{L}_{21} A_k^1(1) \rangle}{\langle A_k^1(1) \widehat{L}_{12} \widehat{L}_{21} A_k^1(1) \rangle}.$$

600 To obtain the finite-difference kinetic equation for the
601 normalized event memory function of first order and, fur-
602 ther, for the higher $(s-1)$ th orders as well, we have to re-
603 peat the foregoing procedure step-by-step. However, we
604 shall make use of the Gram-Schmidt orthogonalization
605 procedure [16]:

$$606 \quad \langle \mathbf{W}_s \mathbf{W}_p \rangle = \delta_{sp} \langle |\mathbf{W}_s|^2 \rangle. \quad (58)$$

607 Where δ_{sp} is a Kronecker's symbol. Now we shall de-
608 rive the recurrence formula $\mathbf{W}_s = \mathbf{W}_s(n)$ for defining the
609 set of the orthogonal dynamic variables:

$$610 \quad \begin{aligned} \mathbf{W}_0 &= \mathbf{A}_k^1, \\ \mathbf{W}_1 &= \{i\widehat{L} - \lambda_1\} \mathbf{W}_0, \\ \mathbf{W}_2 &= \{i\widehat{L} - \lambda_2\} \mathbf{W}_1 - \Lambda_1 \mathbf{W}_0, \dots \end{aligned} \quad (59)$$

611 According to the foregoing formulas we can introduce
612 the succession of projection operators $\Pi_s = \Pi_1^{(s)}$ and the
613 set of mutually complementary projectors $P_s = 1 - \Pi_s$,
614 which possess the following properties:

$$615 \quad \begin{aligned} \Pi_s &= \frac{|\mathbf{W}_s\rangle\langle \mathbf{W}_s|}{\langle |\mathbf{W}_s|^2 \rangle}, & \Pi_s^2 &= \Pi_s, \\ P_s^2 &= P_s, & \Pi_s P_s &= P_s \Pi_s = 0, \\ \Pi_s P_p &= \delta_{sp} \Pi_s, & P_s P_p &= \delta_{sp} P_s. \end{aligned}$$

616 Each of these operators pairs Π_s, P_s splits the corre-
617 sponding Euclidean vector space \mathbf{W}_s into the two mutual
618 complementary subspaces: $W_s = W'_s + W''_s$, $W'_s = \Pi_s W_s$,
619 $W''_s = P_s W_s$. Using the projection operator technique for
620 the next orthogonal variables \mathbf{W}_s , we shall obtain the chain
621 of interconnected kinetic finite-difference equations of the
622 non-Markov type for the normalized correlation functions
623 of the $(s-1)$ th order:

$$\begin{aligned} \frac{\Delta M_1(n)}{\Delta n} &= i\lambda_2 M_1(n) - \Lambda_2 \sum_{j=1}^m M_2(j) M_1(n-j), \\ &\dots, \\ \frac{\Delta M_{s-1}(n)}{\Delta n} &= i\lambda_s M_{s-1}(n) - \Lambda_s \sum_{j=1}^m M_{s-1}(j) M_s(n-j). \end{aligned} \quad (60)$$

624 In these equations the normalized events memory func-
625 tion of the first order: $M_1(n) = \langle \mathbf{W}_1 (1 + i\Delta n \widehat{L})^m \mathbf{W}_1 \rangle /$
626 $\langle |\mathbf{W}_1|^2 \rangle$, memory function of the $(s-1)$ th order: $M_{s-1}(n)$
627 $= \langle \mathbf{W}_{s-1} (1 + i\Delta n \widehat{L})^m \mathbf{W}_{s-1} \rangle / \langle |\mathbf{W}_{s-1}|^2 \rangle$, the proper value
628 of the Liouville's quasioperator \widehat{L} : $\lambda_s = \langle \mathbf{W}_s \widehat{L} \mathbf{W}_s \rangle / \langle |\mathbf{W}_s|^2 \rangle$
629 and the relaxation parameter $\Lambda_s = \langle |\mathbf{W}_s|^2 \rangle / \langle |\mathbf{W}_{s-1}|^2 \rangle$ are
630 introduced.
631

632 The foregoing finite-difference kinetic Eqs. (60) pre-
633 sent the generalization of the statistical theory [31,32,35]
634 for the case of event correlations in discrete stochastic evo-
635 lution of non-Hamilton complex systems.

636 Information Measures of Memory 637 in Complex Systems

638 As an information measures of memory it is useful to ap-
639 ply different dimensionless quantifiers. As a first measure
640 we use the frequency dependence of non-Markovity pa-
641 rameter. This measure was introduced in [31] and it is de-
642 fined as:

$$643 \quad \varepsilon_i(\nu) = \left\{ \frac{\mu_{i-1}(\nu)}{\mu_i(\nu)} \right\}^{1/2}. \quad (61)$$

644 Here, $\mu_i(\nu)$ denotes the frequency power spectrum
645 of memory function of the i th order $M_i(n)$: $\mu_i(\nu) =$
646 $|\Delta n \sum_{n=1}^N M_i(n) \cos(2\pi n\nu)|^2$. The non-Markovity pa-
647 rameter $\varepsilon_i(\nu)$ along with the memory functions enables
648 us to characterize quantitatively the statistical memory ef-
649 fects in discrete complex systems of various nature. Be-
650 cause the functions $\mu_i(\nu)$ exist for each of the i th levels
651 of relaxation, we obtain the statistical spectrum of param-
652 eters: $\varepsilon_i(\nu)$, $i = 1, 2, 3, \dots$

653 Alternatively, a study of ‘memory’ in physiolog- 699
 654 ical time series for electroencephalographic (EEG) 700
 655 and magnetoencephalographic (MEG) signals, both of 701
 656 healthy subjects and patients (including epilepsy patients) 702
 657 has been based on the detrended-fluctuation analysis 703
 658 (DFA) [39,40]. 704

659 The characterization of memory *per se* is based on a set 705
 660 of dimensionless statistical quantifiers which are capable 706
 661 for measuring the memory strength which is inherent to 707
 662 the complex dynamics. 708

663 According to [41] a second set an information memory 709
 664 measure can be constructed as follows: 710

$$665 \quad \delta_i(\nu) = \left| \frac{\tilde{M}'_i(\nu)}{\tilde{M}'_{i+1}(\nu)} \right|.$$

666 Here, $\mu_i(\nu) = |\tilde{M}_i(\nu)|^2$ denotes the power spec- 711
 667 trum of the corresponding memory function $M_i(t)$, 712
 668 $\tilde{M}'_i(\nu) = d\tilde{M}_i(\nu)/d\nu$ and $\tilde{M}_i(\nu)$ is the Fourier trans- 713
 669 form of the memory function $M_i(t)$. The measures $\varepsilon_i(\nu)$ are 714
 670 suitable for the quantification of the memory effects on 715
 671 a relative scale whereas the second set $\delta_i(\nu)$ proves to be 716
 672 useful for quantifying the amplification of relative mem- 717
 673 ory effects occurring on different complexity levels. Both 718
 674 measures provide statistical criteria for comparison be- 719
 675 tween the relaxation time scales and memory time scales 720
 676 of the process under consideration. For values obeying 721
 677 $\{\varepsilon, \delta\} \gg 1$ one can observe a complex dynamics charac- 722
 678 terized by the short-ranged temporal memory scales. In the 723
 679 memoryless limit these processes assume a δ -like mem- 724
 680 ory with parameters $\varepsilon, \delta \rightarrow \infty$. When $\{\varepsilon, \delta\} > 1$ one deals 725
 681 with a situation with moderate memory strength, and the 726
 682 case where both $\varepsilon, \delta \sim 1$ typically constitutes a more regu- 727
 683 lar and robust random process exhibiting strong memory 728
 684 features. 729

685 **Manifestation of Strong Memory** 686 **in Complex Systems**

687 A fundamental role of the strong and weak memory in 730
 688 the functioning of the human organism and seismic phe- 731
 689 nomena can be illustrated by the example of some situa- 732
 690 tions examined next. We will consider some examples of 733
 691 the time series for both living and for seismic systems. It 734
 692 is necessary to note that a comprehensive analysis of the 735
 693 experimental data includes the calculation and the pre- 736
 694 sentation of corresponding phase portraits in some planes 737
 695 of the dynamic orthogonal variables, the autocorrelation 738
 696 time functions, the memory time functions and their fre- 739
 697 quency power spectra, etc. However, we start out by cal- 740
 698 culating two statistical quantifiers, characterizing two in- 741

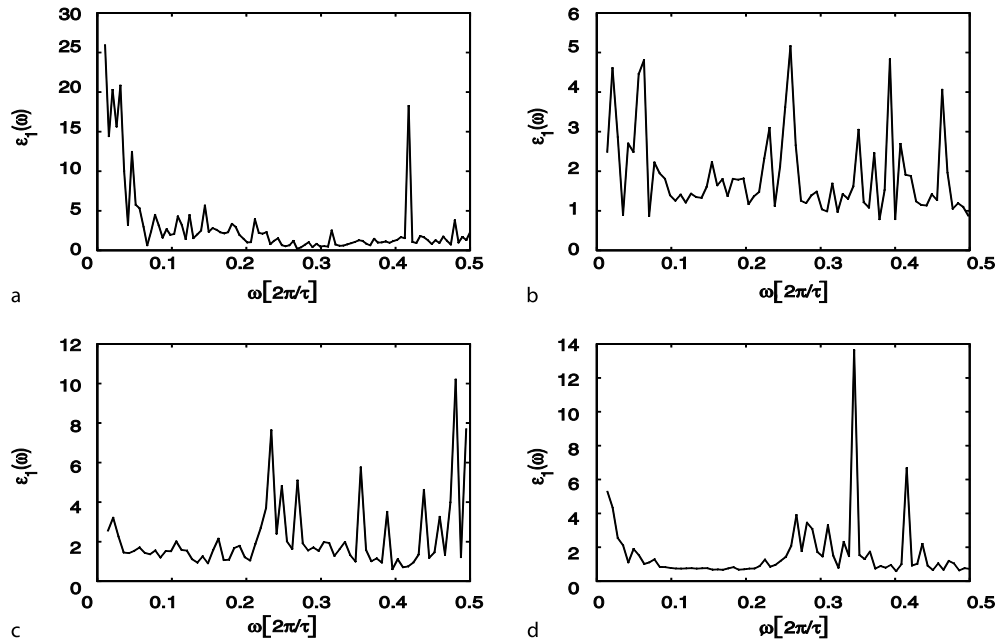
formational measures of memory: the parameters $\varepsilon_1(\omega)$ 699
 and $\delta_1(\omega)$. 700

701 Figures 1 and 3 present the results of experimental 702
 703 data of pathological states of human cardiovascular sys- 704
 705 tems (CVS). Figure 2 depicts the analysis for the seismic 706
 707 observation. Figures 4 and 5 indicate the memory effects 708
 709 for the patients with Parkinson disease (PD), and the last 710
 711 two Figs. 6, 7 demonstrate the key role of the strength of 712
 713 memory in the case of time series of patients suffering 714
 715 from photosensitive epilepsy which are contrasted with 716
 717 signals taken from healthy subjects. All these cases con- 718
 719 vincingly display the crucial role of the statistical memory 720
 721 in the functioning of complex (living and seismic) systems. 722

723 A characteristic role of the statistical memory can be 724
 725 detected from Fig. 1 for the typical representatives taken 726
 727 from patients from four different CVS-groups: (a) for 728
 729 healthy subject, (b) for a patient with rhythm driver mi- 729
 730 gration, (c) for a patient after myocardial infarction (MI), 730
 731 (d) for a patient after MI with subsequent sudden car- 731
 732 diac death (SSCD). All these data were obtained from the 732
 733 short time series of the dynamics of RR-intervals from the 733
 734 electric signals of the human ECG’s. It can be seen here 734
 735 that significant memory effects typically lead to the long- 735
 736 time correlations in the complex systems. For healthy we 736
 737 observe weak memory effects while and large values of 737
 738 the measure memory $\varepsilon_1(\omega = 0) \approx 25$. The strong mem- 738
 739 ory and the long memory time (approximately, 10 times 739
 740 more) are being observed with the help of 3 patient groups: 740
 741 with RDM (rhythm driver migration) (b), after MI (c) and 741
 742 after MI with SSCD (d). 742

729 Figure 2 depicts the strong memory effects presented 729
 730 in seismic phenomena. By a transition from the steady 730
 731 state of Earth ((a), (b) and (c)) to the state of strong earth- 731
 732 quake (EQ) ((d), (e), and (f)) a remarkable amplification 732
 733 of memory effects is highly visible. The term amplification 733
 734 refers to the appearance of strong memory and the prolon- 734
 735 gation of the memory correlation time in the seismic sys- 735
 736 tem. Recent study show that discrete non-Markov stochas- 736
 737 tic processes and long-range memory effects play a cru- 737
 738 cial role in the behavior of seismic systems. An approach, 738
 739 permitting us to obtain an algorithm of strong EQ fore- 739
 740 casting and to differentiate technogenic explosions from 740
 741 weak EQs, can be developed thereupon. 741

742 Figure 3 demonstrates an intensification of memory 742
 743 effects of one order at the transition from healthy people 743
 744 ((a), (b) and (c)) to patient suffering from myocardial in- 744
 745 farction. The figures were calculated from the long time se- 745
 746 ries of the RR-intervals dynamics from the human ECG’s. 746
 747 The zero frequency values $\varepsilon_1(\omega = 0)$ at $\omega = 0$ sharply re- 747
 748 duced, approximately of the size of one order for patient 748
 749 as compared to healthy subjects. 749



Correlations in Complex Systems, Figure 1

Frequency spectrum of the first information measure of memory (first point in the statistical spectrum on non-Markovity parameter) $\varepsilon_1(\omega)$ for the fourth cardiac patient groups from the short time series of RR-intervals: healthy subject (a), patient with rhythm driver migration (RDM) (b), patient after myocardial infarction (MI) (c), and patient after MI with subsequent sudden cardiac death (SCD) (d). The frequency is marked in terms of units of τ^{-1} . All spectra reveal the miscellaneous faces of statistical memory's strength. For the healthy subject one can see Markov effects and weak memory. For other three cases of cardiac diseases we note the diverse displays of strong memory. The strong memory has been accompanied by the spikes of the weak memory: for RDM on the all frequency regions, for patient with MI for the middle and high frequencies and for patient after MI with SSCD only for high frequencies. From Fig. 7 in [104]

750 Figures 4 and 5 illustrate the behavior for patients with
 751 Parkinson's disease. Figure 4 shows time recording of the
 752 pathological tremor velocity in the left index finger of
 753 a patient with Parkinson's disease (PD) for eight diverse
 754 pathological cases (with or without medication, with or
 755 without deep brain stimulation (DBS), for various DBS,
 756 medication and time conditions). Figure 5, arranged in
 757 accordance with these conditions, displays a wide variety
 758 of the memory effects in the treatment of PD's patients.
 759 Due to the large impact of memory effects this observa-
 760 tion permits us to develop an algorithm of exact diagnosis
 761 of Parkinson's disease and a calculation of the quantita-
 762 tive parameter of the quality of treatment. A physical role
 763 of the strong and long memory correlation time enables
 764 us to extract a vital information about the states of vari-
 765 ous patient on basis of notions of correlation and memory
 766 times.

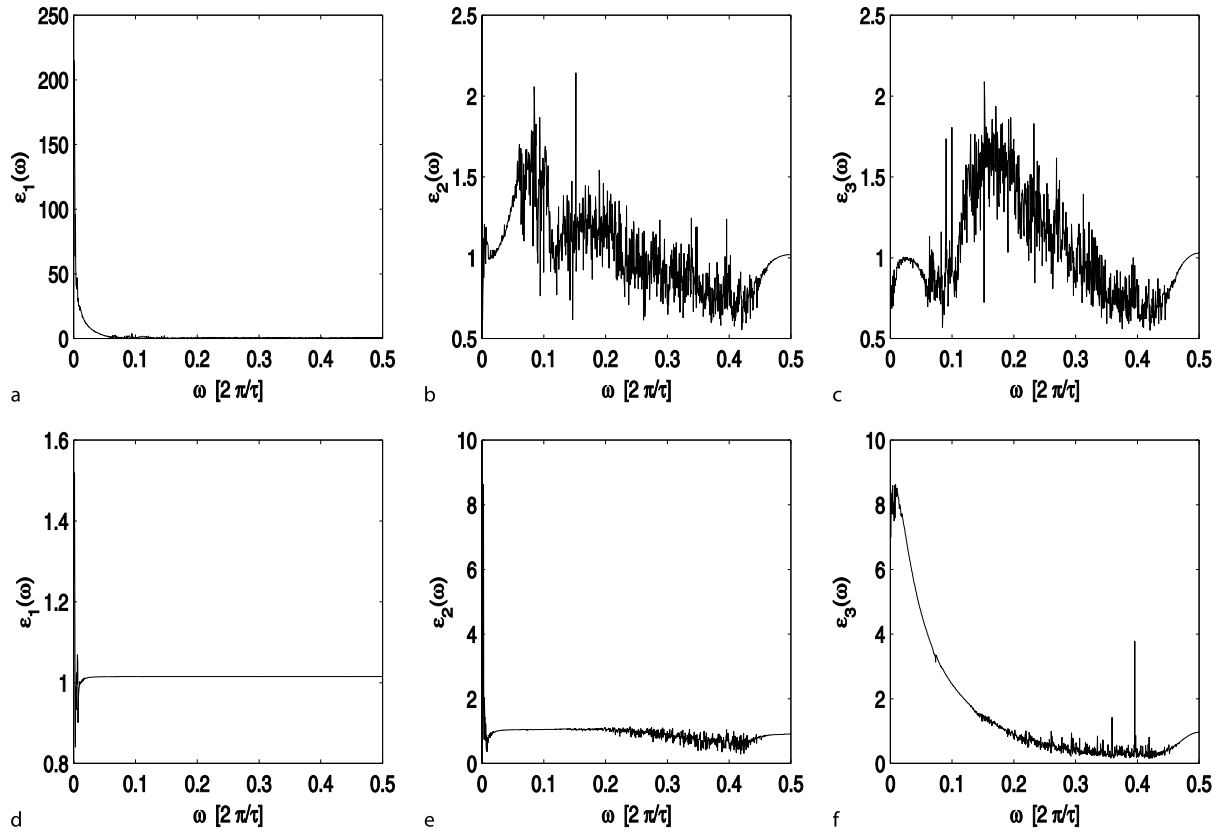
767 According to Figs. 6 and 7 specific information
 768 about the physiological mechanism of photosensitive
 769 epilepsy (PSE) was obtained from the analysis of the strong
 770 memory effects via the registration the neuromagnetic

771 responses in recording of magnetoencephalogram (MEG)
 772 of the human brain core. Figure 6 presents the topographic
 773 dependence of the first level of the second memory mea-
 774 sure $\delta_1(\omega = 0; n)$ for the healthy subjects in the whole
 775 group (upper line) vs. patients (lower line) for red/blue
 776 combination of the light stimulus. This topographic de-
 777 pendence of $\varepsilon_1(\omega = 0; n)$ depicted in Fig. 6 clearly demon-
 778 strates the existence of long-range time correlation. It is
 779 accompanied by a sharp increase of the role of the statisti-
 780 cal memory effects in the all MEG's sensors with sensor
 781 numbers $n = 1, 2, \dots, 61$ of the patient with PSE in com-
 782 parison with healthy peoples. A sizable difference between
 783 the healthy subject and a subject with PSE occurs.

784 To emphasize the role of strong memory one can conti-
 785 nue studying the topographic dependence in terms of the
 786 novel informational measure, the index of memory, de-
 787 fined as:

$$788 \nu(n) = \frac{\delta_1^{\text{healthy}}(0; n)}{\delta_1^{\text{patient}}(0; n)}, \quad (62)$$

789 see in Fig. 7.



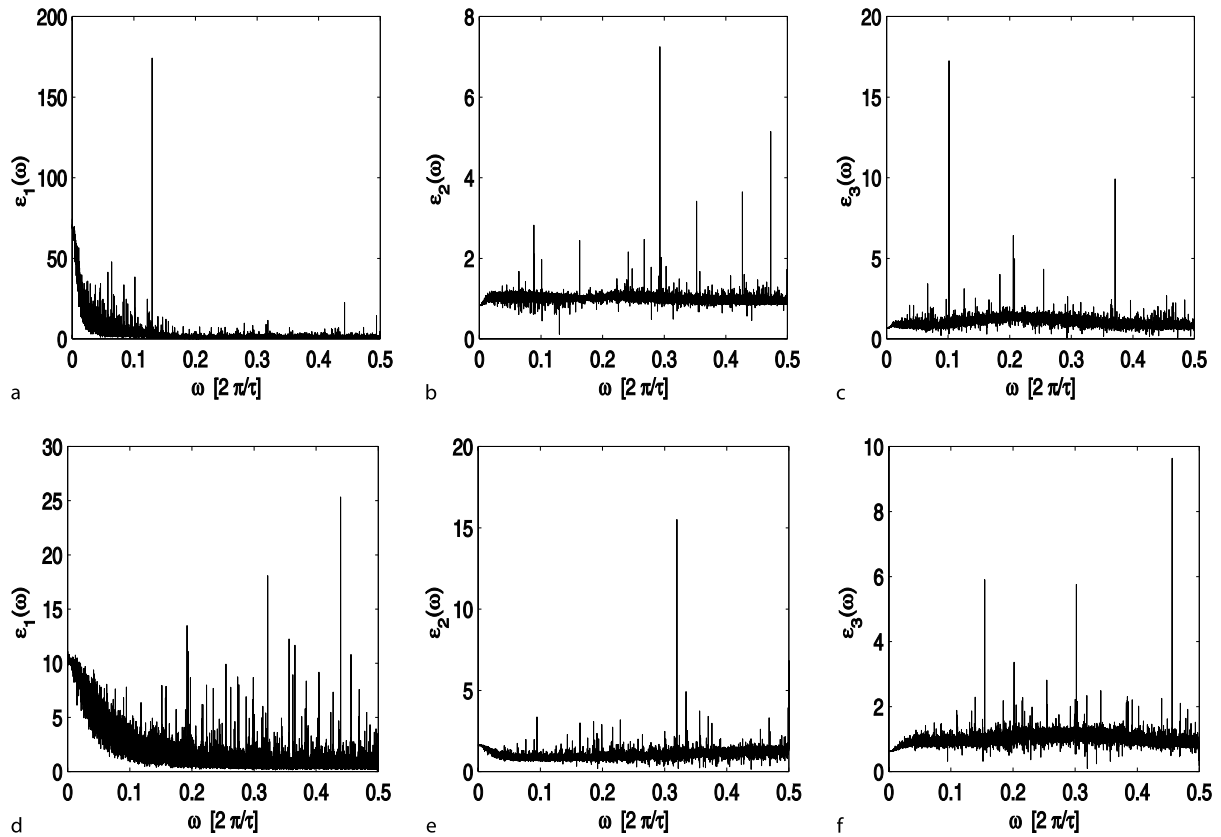
Correlations in Complex Systems, Figure 2

Frequency spectra of the first three points of the first measure of memory (non-Markovity parameters) $\varepsilon_1(\omega)$, $\varepsilon_2(\omega)$, and $\varepsilon_3(\omega)$ for the seismic phenomena: a, b, c long before the strong Earthquake (EQ) for the steady state of Earth and d, e, f during the strong EQ. Markov and quasi-Markov behavior of seismic signals with manifestation of the weak memory is observed only for ε_1 in state before the strong EQ. All remaining cases b, c, d and e relate to non-Markov processes. Strong non-Markovity and strong memory is typical for case d (state during the strong EQ). In behavior of $\varepsilon_2(\omega)$ and $\varepsilon_3(\omega)$ one can see a transition from quasi-Markovity (at low frequencies) to strong non-Markovity (at high frequencies). From Fig. 6 in [105]

790 This measure quantifies the detailed memory effects
 791 in the individual MEG sensors of the patient with PSE
 792 versus the healthy group. A sharp increase of the role
 793 of the memory effects in the stochastic behavior of the
 794 magnetic signals is clearly detected in sensor numbers
 795 $n = 10, 46, 51, 53$ and 59 . The observed points of MEG
 796 sensors locate the regions of a protective mechanism
 797 against PSE in a human organism: frontal (sensor 10),
 798 occipital (sensors 46, 51 and 53) and right parietal (sen-
 799 sor 59) regions. The early activity in these sensors may re-
 800 flect a protective mechanism suppressing the cortical hy-
 801 peractivity due to the chromatic flickering.

802 We remark that some early steps towards understand-
 803 ing the normal and various catastrophic states of com-
 804 plex systems have already been taken in many fields of
 805 science such as cardiology, physiology, medicine, neuro-
 806 logy, clinical neurophysiology, neuroscience, seismology

and so forth. With the underlying systems showing frac- 807
 tal and complicated spatial structures numerous studies 808
 applying the linear and nonlinear time series analysis to 809
 various complex systems have been discussed by many 810
 authors. Specifically the results obtained shows evidence 811
 of the significant nonlinear structure evident in the reg- 812
 istered signals in the control subjects, whereas nonlinear- 813
 ity for the patients and catastrophic states were not de- 814
 tected. Moreover the couplings between distant parts and 815
 regions were found to be stronger for the control subjects. 816
 These prior findings are leading to the hypothesis that the 817
 real normal complex systems are mostly equipped with 818
 significantly nonlinear subsystems reflecting an inherent 819
 mechanism which stems against a synchronous excitation 820
 vs. outside impact or inside disturbances. Such nonlinear 821
 mechanisms are likely absent in the occurrence of catas- 822
 trophical or pathological states of the complex systems. 823



Correlations in Complex Systems, Figure 3

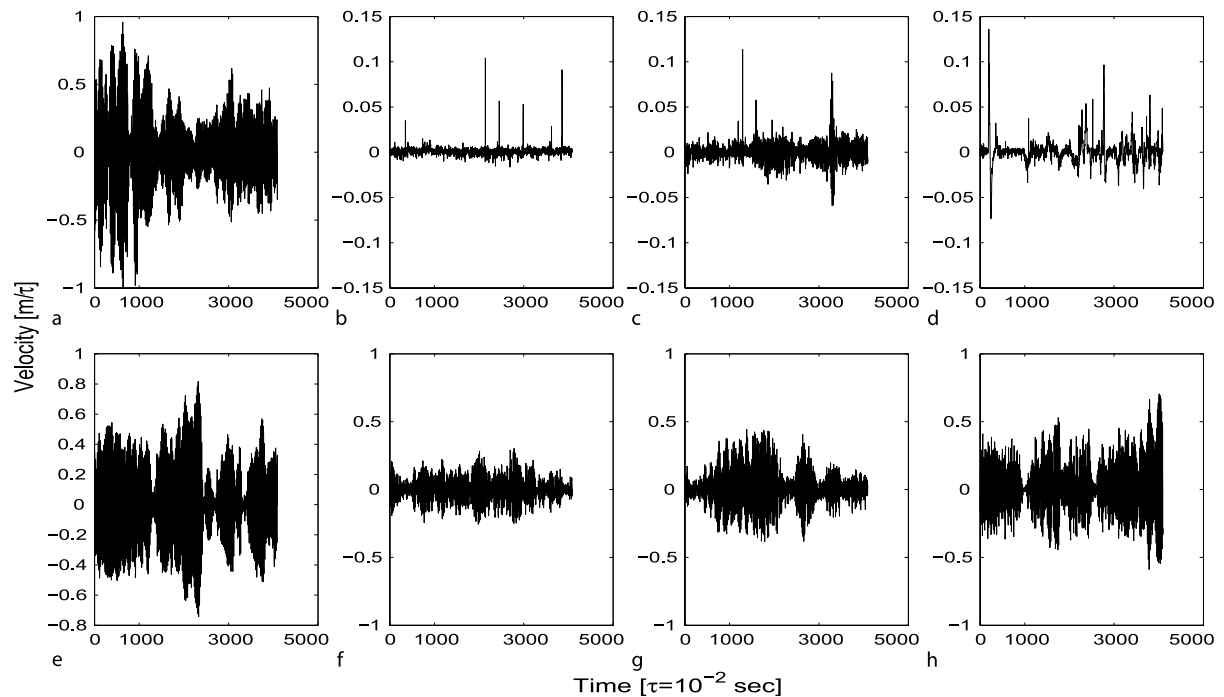
The frequency dependence of the first three points of non-Markovity parameter (NMP) for the healthy person (a), (b), (c) and patient after myocardial infarction (MI) (d), (e), (f) from the time dynamics of RR-intervals of human ECG's for the case of the long time series. In the spectrum of the first point of NMP $\varepsilon_1(\omega)$ there is an appreciable low-frequency (long time) component, which concerns the quasi-Markov processes. Spectra NMP $\varepsilon_2(\omega)$ and NMP $\varepsilon_3(\omega)$ fully comply with non-Markov processes within the whole range of frequencies. From Fig. 6 in [106]

824 From the physical point of view our results can be used
 825 as a toolbox for testing and identifying the presence or absence
 826 of various memory effects as they occur in complex
 827 systems. The set of our memory quantifiers is uniquely associated
 828 with the appearance of memory features in the chaotic behavior
 829 of the observed signals. The registration of the behavior belonging
 830 to these indicators, as elucidated here, is of beneficial use for
 831 detecting the catastrophic or pathological states in the complex
 832 systems. There exist alternative quantifiers of different nature
 833 as well, such as the Lyapunov's exponent, Kolmogorov-Sinai
 834 entropy, correlation dimension, etc., which are widely used in
 835 nonlinear dynamics and relevant applications. In the present
 836 context, we have found out that the employed memory
 837 measures are not only convenient for the analysis but are
 838 also ideally suitable for the identification of anomalous
 839 behavior occurring in complex systems. The search for other
 840 quantifiers, and foremost, the ways of optimization of such

842 measures when applied to the complex discrete time
 843 dynamics presents a real challenge. Especially this objective
 844 is met when attempts are made towards the identification
 845 and quantification of functioning in complex systems. This
 846 work presents initial steps towards the understanding of basic
 847 foundation of anomalous processes in complex systems on the
 848 basis of a study of the underlying memory effects and connected
 849 with this, the occurrence of long lasting correlations. 850

851 **Some Perspectives on the Studies of Memory** 852 **in Complex Systems**

853 Here we present a few outlooks on the fundamental role
 854 of statistical memory in complex systems. This involves
 855 the issue of studying cross-correlations. The statistical theory
 856 of stochastic dynamics of cross-correlation can be created
 857 on the basis of the mentioned formalism of projection



Correlations in Complex Systems, Figure 4

Pathological tremor velocity in the left index finger of the sixth patient with Parkinson's disease (PD). The registration of Parkinsonian tremor velocity is carried out for the following conditions: **a** "OFF-OFF" condition (no any treatment), **b** "ON-ON" condition (using deep brain stimulation (DBS) by electromagnetic stimulator and medicaments), **c** "ON-OFF" condition (DBS only), **d** "OFF-ON" condition (medicaments (L-Dopa) only), **e-h** the "15 OFF", "30 OFF", "45 OFF", "60 OFF" conditions – the patient's states 15 (30, 45, 60) minutes after the DBS is switched off, no treatment. Let's note the scale of the pathological tremor amplitude (see the vertical scale). Such representation of the time series allows us to note the increase or the decrease of pathological tremor. From Fig. 1 in [107]

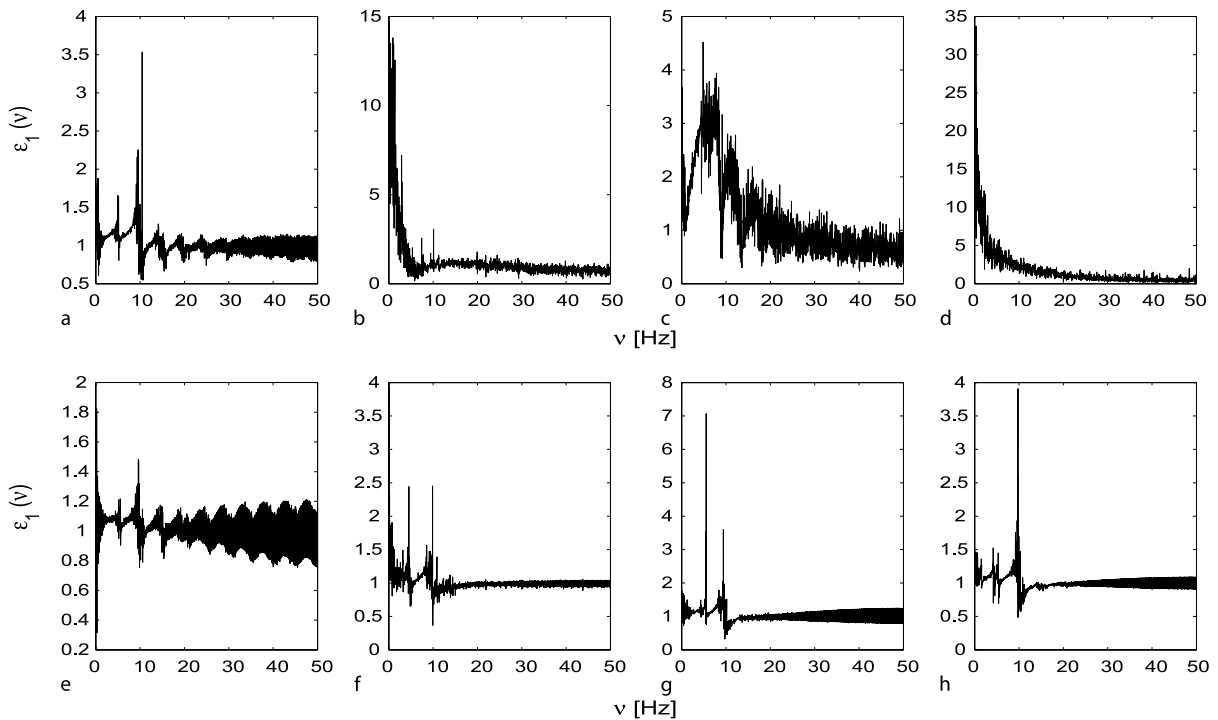
858 operators technique in the linear space of random vari- 879
 859 ables. As a result we obtain the cross-correlation memory 880
 860 functions (MF's) revealing the statistical memory effects in 881
 861 complex systems. Some memory quantifiers will appear sim- 882
 862 ultaneously which will reflect cross-correlation between 883
 863 different parts of CS. Cross-correlation MF's can be very 884
 864 useful for the analysis of the weak and strong interactions, 885
 865 signifying interrelations between the different groups of 886
 866 random variables in CS. Besides that the cross-correlation 887
 867 can be important for the problem of phase synchroniza- 888
 868 tion, which can find a unique way of studying of synchro- 889
 869 nization phenomena in CS that has a special importance 890
 870 when studying aspects of brain and living systems dynam- 891
 871 ics. 892

872 Some additional information about the strong and 893
 873 weak memory effects can be extracted from the observa- 894
 874 tion of correlation in CS in the random event's scales. 895
 875 Similar effects are playing a crucial role in the differen- 896
 876 tiation between stochastic phenomena within astrophys- 897
 877 ical systems, for example, in galaxies, pulsars, quasars, mi- 898
 878 croquasars, lacertides, black holes, etc. One of the most 899

important area of application of developed approach is 879
 a bispectral and polyspectral analysis for the diverse CS. 880
 From the mathematical point of view a correct definition 881
 of the spectral properties in the functional space of ran- 882
 dom functions is quite important. A variety of MF's arises 883
 in the quantitative analysis of the fine details of memory 884
 effects in a nonlinear manner. The quantitative control of 885
 the treatment quality in the diverse areas of medicine and 886
 physiology may be one of the important biomedical appli- 887
 cation of the manifestation of the strong memory effects. 888

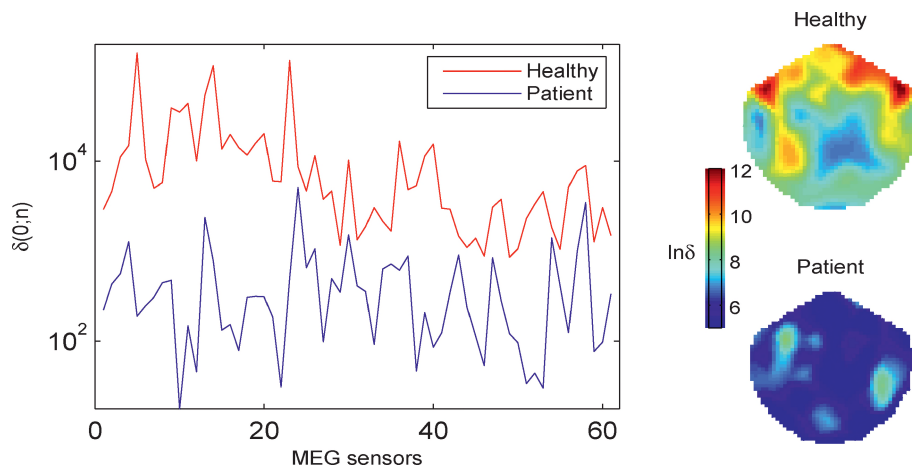
889 These and other features of memory effects in CS call 890
 for an advanced development of brain studies on the ba- 891
 sis of EEG's and MEG's data, cardiovascular, locomotor 892
 and respiratory human systems, in the development of the 893
 control system of information flows in living systems. An 894
 example is the prediction of strong EQ's and the clear dif- 895
 ferentiation between the occurrence of weak EQ's and the 896
 technogenic explosions, etc. 897

898 In conclusion, we hope that the interested reader 899
 becomes invigorated by this presentation of correlation 900
 and memory analysis of the inherent nonlinear system 901



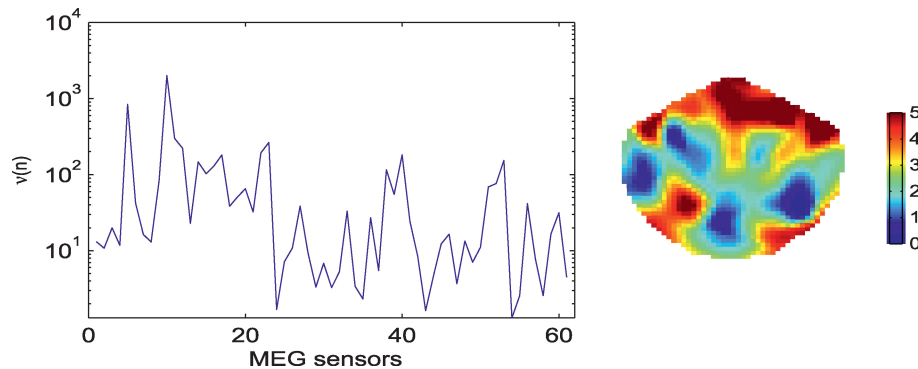
Correlations in Complex Systems, Figure 5

The frequency dependence of the first point of the non-Markovity parameter $\varepsilon_1(\nu)$ for pathological tremor velocity in the patient. As an example, the sixth patient with Parkinson's disease is chosen. The figures are submitted according to the arrangement of the initial time series. The characteristic low-frequency oscillations are observed in frequency dependence (a, e–h), which get suppressed under medical influence (b–d). The non-Markovity parameter reflects the Markov and non-Markov components of the initial time signal. The value of the parameter on zero frequency $\varepsilon_1(0)$ reflects the total dynamics of the initial time signal. The maximal values of parameter $\varepsilon_1(0)$ correspond to small amplitudes of pathological tremor velocity. The minimal values of this parameter are characteristic of significant pathological tremor velocities. The comparative analysis of frequency dependence $\varepsilon_1(\nu)$ allows us to estimate the efficiency of each method of treatment. From Fig. 5 in [107]



Correlations in Complex Systems, Figure 6

The topographic dependence of the first point of the second measure of memory $\delta_1(\omega = 0; n)$ for the healthy on average in the whole group (*upper line*) vs. patient (*lower line*) for R/B combination of the light stimulus. One can note the singular weak memory effects for the healthy on average in sensors with No. 5, 23, 14, 11 and 9



Correlations in Complex Systems, Figure 7

The topographic dependence of the memory index $\nu(n) = \nu_1(n; 0)$ for the the whole group of healthy on average vs. patient for an R/B combination of the light stimulus. Strong memory in patient vs. healthy appears clearly in sensors with No. 10, 5, 23, 40 and 53

dynamics of varying complexity. He can find further details how significant memory effects typically cause long time correlations in complex systems by inspecting more closely some of the published items in [42–103].

There are the relationships between standard fractional and polyfractal processes and long-time correlation in complex systems, which were explained in [39,40,44,45, 46,49,53,54,60,62,64,76,79,83,84,94] in detail.

Example of using the Hurst exponent over time for testing the assertion that emerging markets are becoming more efficient can be found in [51].

While over 30 measures of complexity have been proposed in the research literature one can distinguish [42,55, 66,81,89,99] with the specific designation of long-time correlation and memory effects.

Methods [48,57] are focused on long range correlation processes that are nonlocal in time and whence show memory effects.

The statistical characterization of the nonstationarities in real-world time series is an important topic in many fields of research and some numerous methods of characterizing nonstationary time series were offered in [59, 65,84].

Long-range correlated time series have been widely used in [52,61,63,68,74] for the theoretical description of diverse phenomena.

Example of the study an anatomy of extreme events in a complex adaptive system can be found in [67].

Approaches for modeling long-time and long-range correlation in complex systems from time series are investigated and applied to different examples in [50,56,69,70, 73,75,80,82,86,100,101,102].

Detecting scale invariance and its fundamental relationships with statistical structures is one of the most relevant problems among those addressed correlation analysis [47,71,72,91].

Specific long-range correlation in complex systems are the object of active research due to its implications in the technology of materials and in several fields of scientific knowledge with the use of quantified histograms [78], decrease of chaos in heart failure [85], scaling properties of ECG's signals fluctuations [87], transport properties in correlated systems [88] etc.

It is demonstrated in [43,92,93] how ubiquity of the long-range correlations is apparent in typical and exotic complex statistical systems with application to biology, medicine, economics and to time clustering properties [95,98].

The scale-dependent wavelet and spectral measures for assessing cardiac dysfunction have been used in [97].

In recent years the study of an increasing number of natural phenomena that appear to deviate from standard statistical distributions has kindled interest in alternative formulations of statistical mechanics [58,101].

At last, papers [77,90] present the samples of the deep and multiple interplay between discrete and continuous long-time correlation and memory in complex systems and the corresponding modeling the discrete time series on the basis of physical Zwanzig–Mori's kinetic equation for the Hamilton statistical systems.

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